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(54) **MACHINE LEARNING SYSTEM FOR ASSESSING HEART VALVES AND SURROUNDING CARDIOVASCULAR TRACTS**

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USPC ..... 706/12  
See application file for complete search history.

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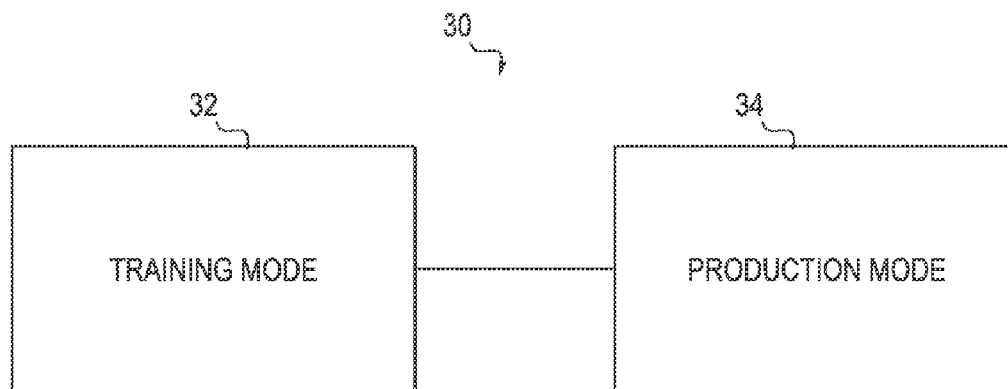
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(57) **ABSTRACT**

A machine learning system for evaluating at least one characteristic of a heart valve, an inflow tract, an outflow tract or a combination thereof may include a training mode and a production mode. The training mode may be configured to train a computer and construct a transformation function to predict an unknown anatomical characteristic and/or an unknown physiological characteristic of a heart valve, inflow tract and/or outflow tract, using a known anatomical characteristic and/or a known physiological characteristic the heart valve, inflow tract and/or outflow tract. The production mode may be configured to use the transformation function to predict the unknown anatomical characteristic and/or the unknown physiological characteristic of the heart valve, inflow tract and/or outflow tract, based on the known anatomical characteristic and/or the known physiological characteristic of the heart valve, inflow tract and/or outflow tract.

**38 Claims, 7 Drawing Sheets**



(51) **Int. Cl.***A61B 5/00* (2006.01)*G06N 5/04* (2006.01)*G06F 19/00* (2011.01)(56) **References Cited**

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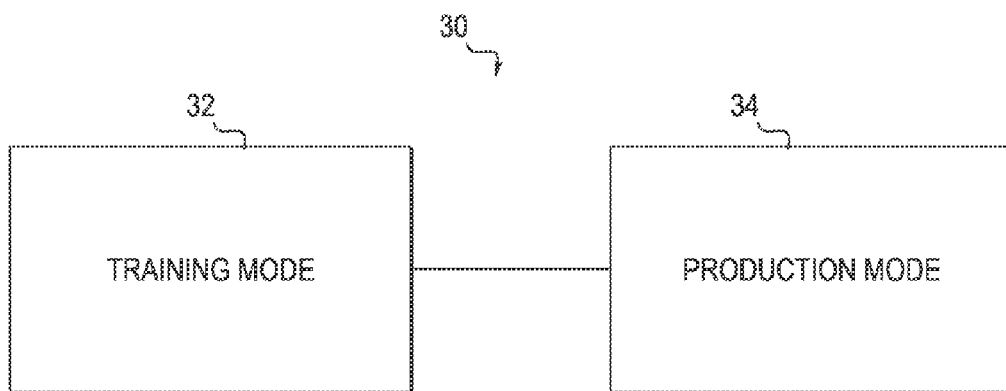


FIG. 1

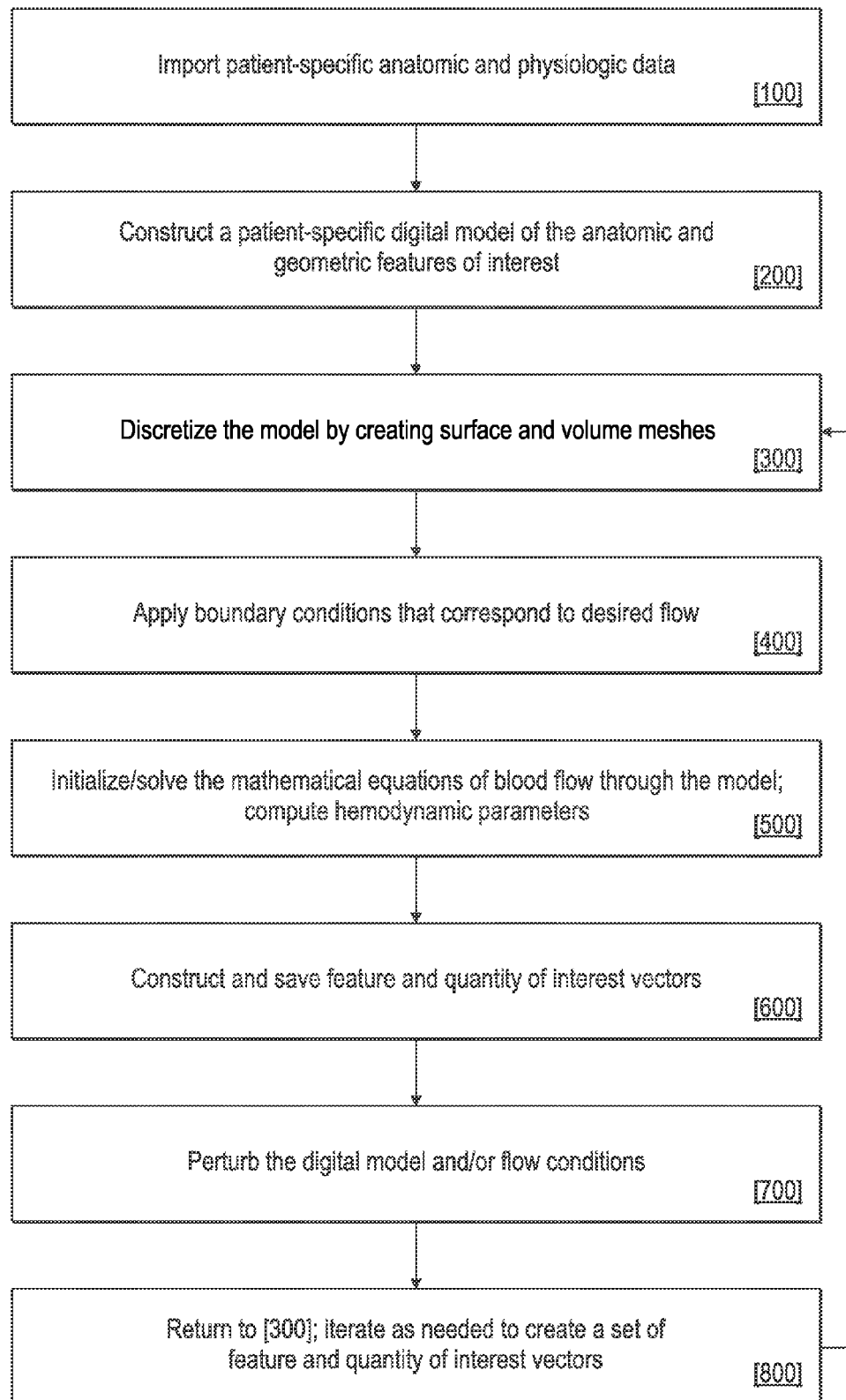


FIG. 2

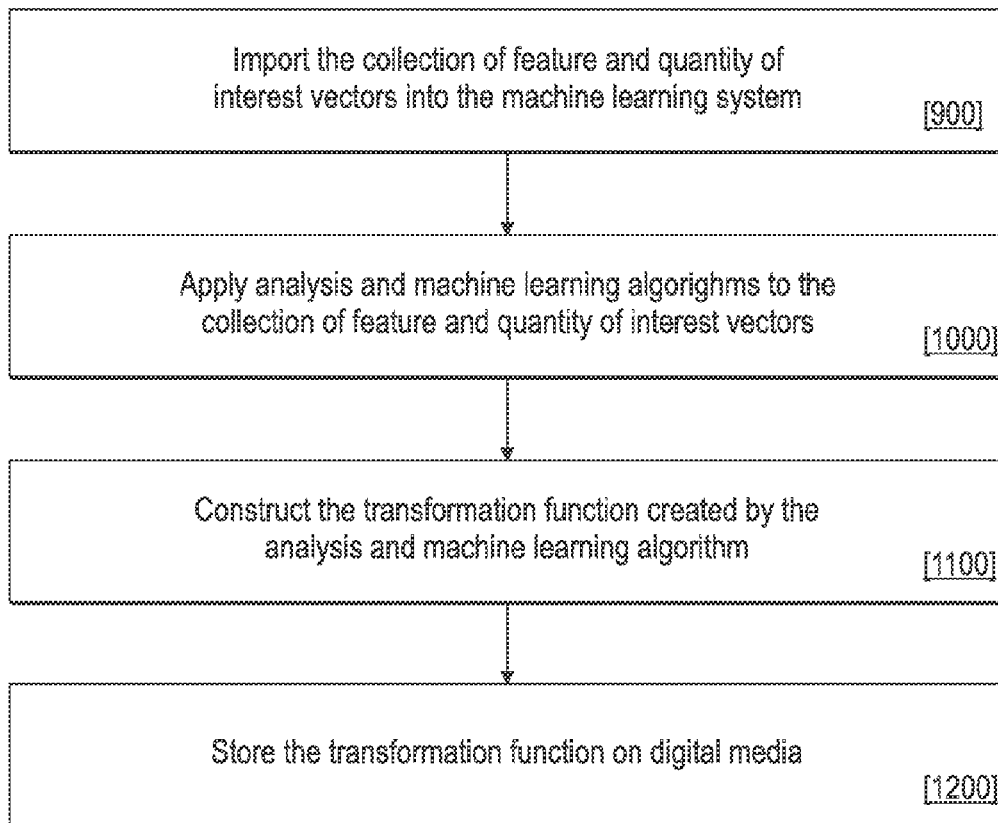


FIG. 3

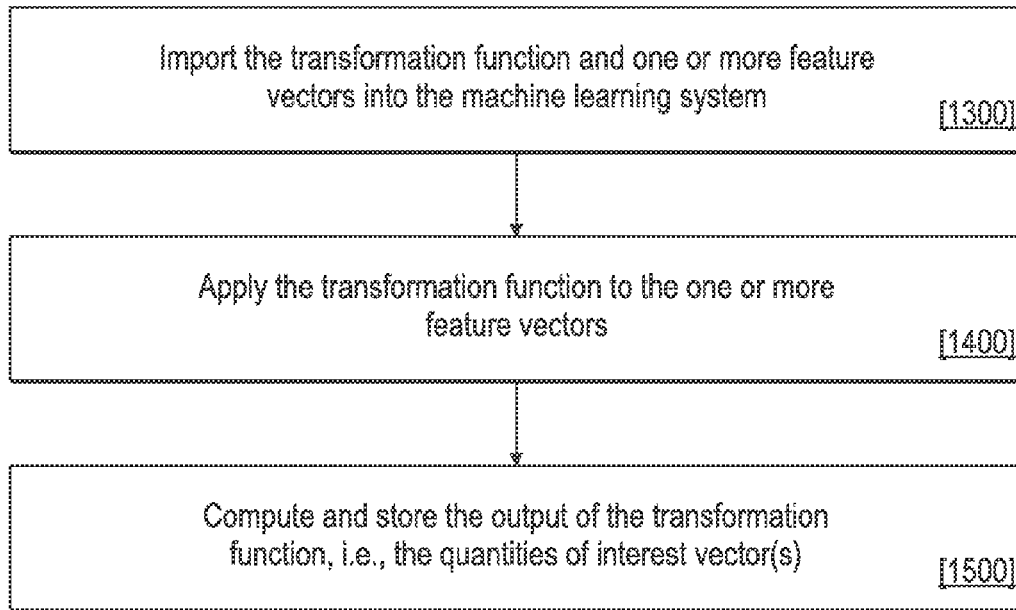


FIG. 4

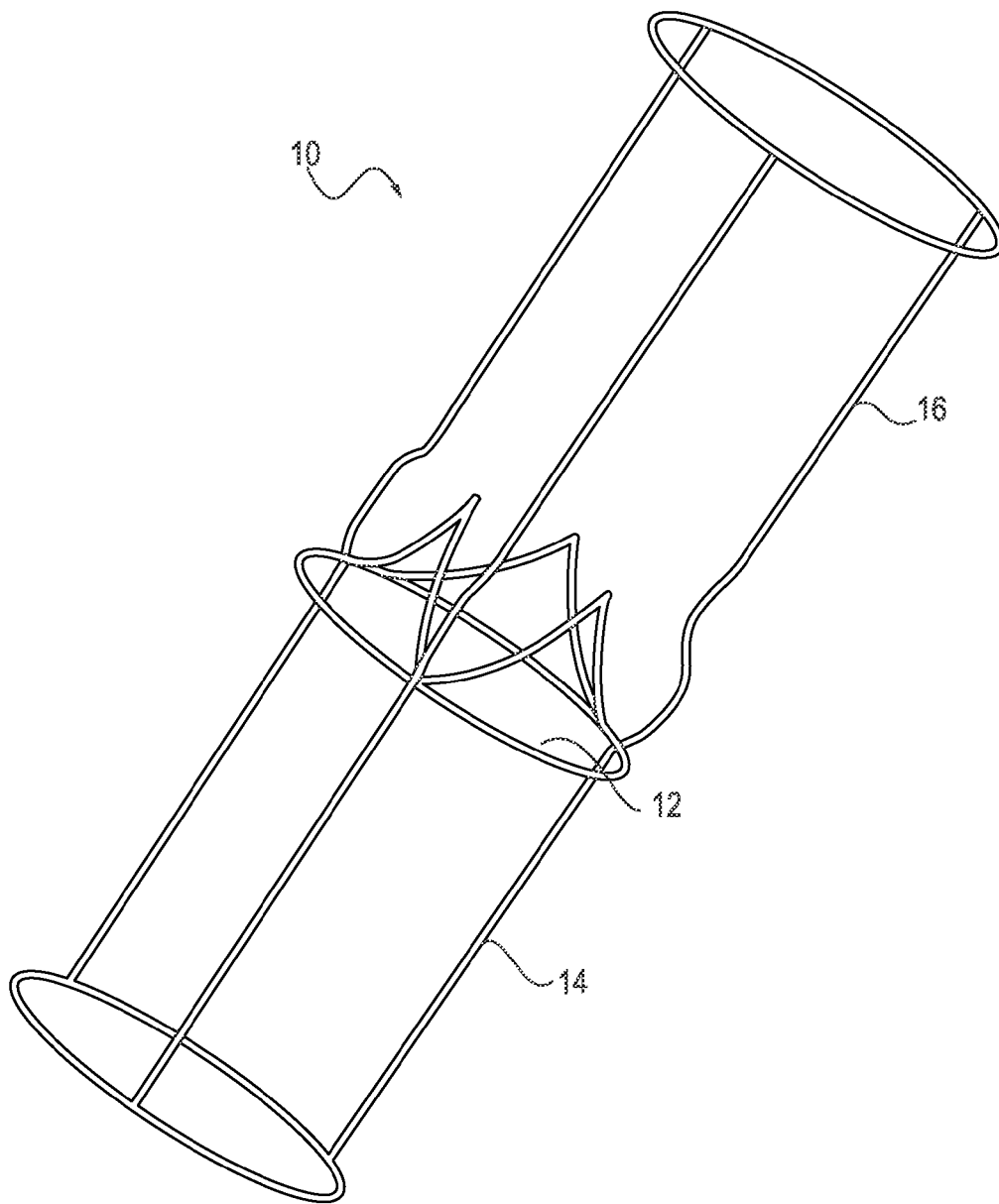


FIG. 5

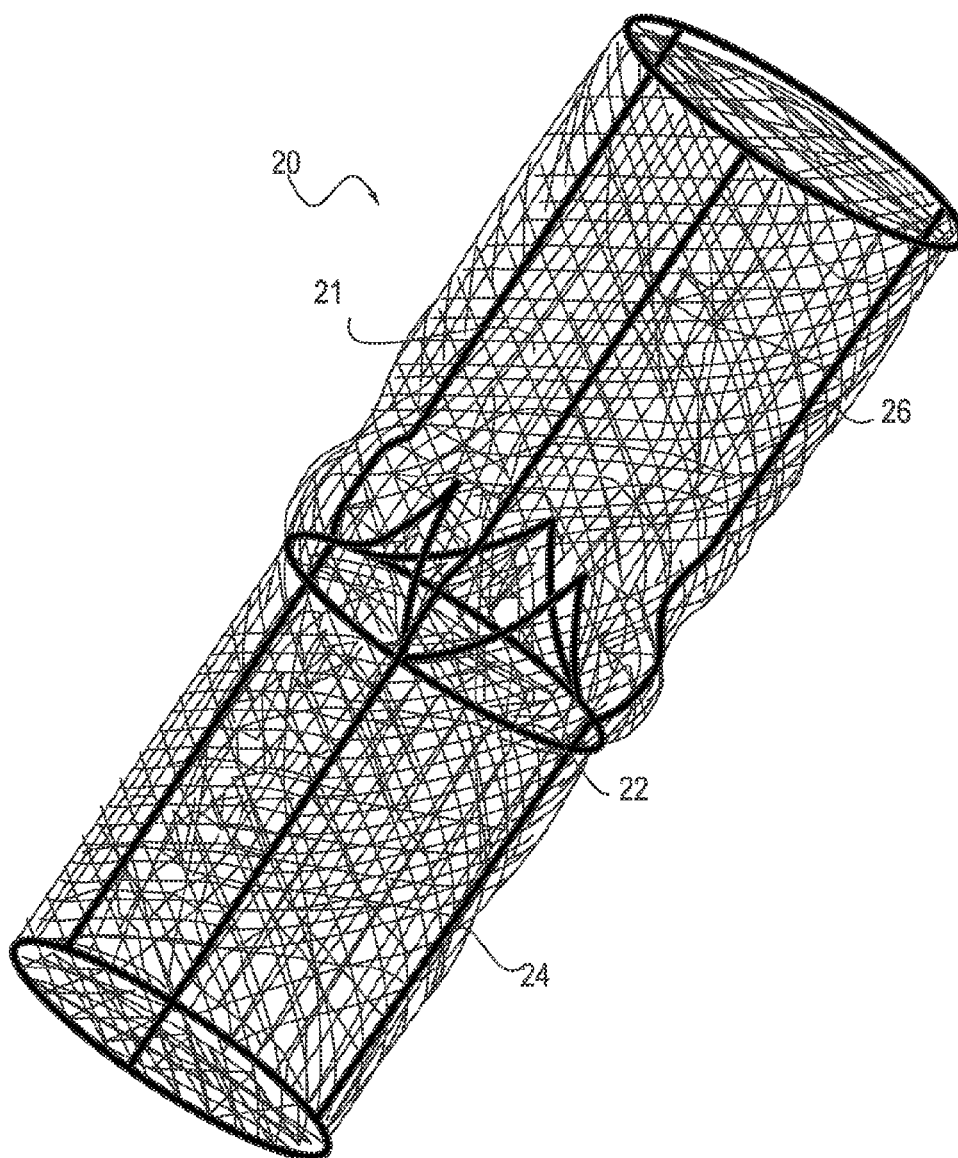


FIG. 6



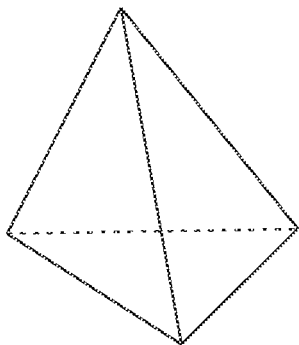


FIG. 7A

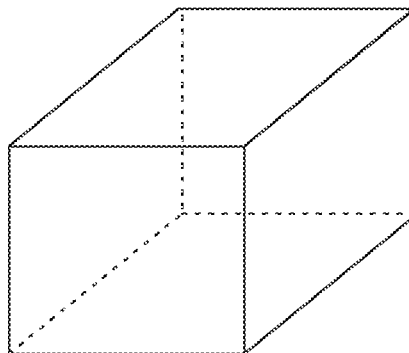


FIG. 7B

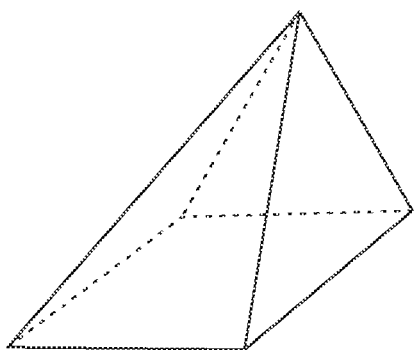


FIG. 7C

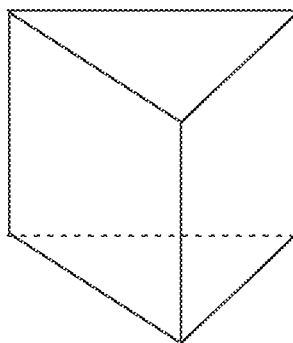


FIG. 7D

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# **MACHINE LEARNING SYSTEM FOR ASSESSING HEART VALVES AND SURROUNDING CARDIOVASCULAR TRACTS**

## **CROSS-REFERENCE TO RELATED APPLICATION**

This application is a continuation application of Ser. No. 14/511,018, now U.S. Pat. No. 9,092,743, filed Oct. 9, 2014, entitled "MACHINE LEARNING SYSTEM FOR ASSESSING HEART VALVES AND SURROUNDING CARDIOVASCULAR TRACTS," which claims priority to U.S. Provisional Patent Application No. 61/894,814, entitled "MACHINE LEARNING SYSTEM FOR ASSESSING HEART VALVES AND SURROUNDING CARDIOVASCULAR TRACTS" filed on Oct. 23, 2013. The full disclosures of the above-listed patent applications are hereby incorporated by reference herein.

## **FIELD**

The present disclosure relates generally to the fields of machine learning, computer modeling and simulation, and computer aided design. More specifically, the disclosure relates to computer-based machine learning systems and methods for constructing and executing models of cardiac anatomy and physiology. These models may be used for therapeutic, treatment, and/or diagnostic purposes.

## **BACKGROUND**

Cardiovascular disease is the leading cause of death in the United States and claims the lives of more than 600,000 Americans each year. According to the American Heart Association (AHA), more than five million Americans are diagnosed with heart valve disease each year, and diseases of the aortic and mitral valves are the most prevalent. Combined, aortic and mitral valve diseases affect more than five percent of the U.S. population.

The proper assessment and diagnosis of heart valve operation and the condition of surrounding cardiovascular tracts are essential for ensuring high quality patient care. To this end, several imaging modalities may be used to inspect the condition and function of heart valves and the surrounding vasculature. Transthoracic and transesophageal echocardiography, for example, use ultrasound technology to create two- and/or three-dimensional images of heart valves and the surrounding inflow/outflow tracts (e.g., left ventricular outflow tract, ascending aorta). Further, computed tomography (CT) and magnetic resonance imaging (MRI) may also be used.

All imaging modalities have strengths and weaknesses that may limit their ability to provide a complete and comprehensive assessment of anatomic and/or physiologic condition. The spatial resolution of echocardiographic images, for example, may inhibit a detailed analysis of functional operation, especially for highly calcified heart valves. Computed tomography may provide higher resolution images than echocardiography, but CT imaging studies are more costly and expose patients to radiation that is potentially harmful. In addition, contrast agents, which may be highly nephrotoxic and may be associated with alterations in renal function, are often used during CT examinations. Hence, new and novel methods that enable an accurate anatomic and physiological assessment of heart valves and

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the surrounding vasculature, while not exposing patients to excessive risks or prohibitive costs, are desirable.

Patients diagnosed with symptomatic and clinically significant heart valve abnormalities may be candidates for valvular repair or replacement. When repair or replacement is indicated, an accurate and complete understanding of valvular anatomy is essential to ensure a favorable outcome. In addition, the anatomic and physiologic characteristics of the inflow and outflow tracts that surround the heart valve(s) must also be understood.

New methods for assessing the anatomic and/or physiologic condition of native and prosthetic heart valves and the surrounding inflow/outflow tracts should enable more accurate and precise treatment planning. These new methods may complement and/or work in conjunction with existing methods, or they may stand alone. Regardless, such technologies must provide clear and demonstrable benefits to the physician(s) who treat patients with heart valve disease and/or diseases of the surrounding cardiac tracts. Further, new technologies must not expose patients to excessive medical risks and should be cost effective.

Therefore, to improve diagnostic and treatment capabilities, it is desirable to have a system for quickly and accurately assessing the physiological function, condition, and morphology of heart valves and the surrounding inflow/outflow tracts, which thereby enables the proper diagnosis of heart valve disease and, if warranted, facilitates treatment planning.

## **DESCRIPTION OF RELATED ART**

There are many academic and industrial research groups that use computer modeling and simulation to analyze flow through heart valves. Historically, valvular hemodynamic analyses have focused on the aortic heart valve and have employed methods of computational fluid dynamics (CFD) to provide detailed insight into the blood flow surrounding the aortic valve. These insights have then been used to facilitate the design and construction of heart valves with desirable hemodynamic properties that maximize functionality and durability while minimizing the potentially fatal risks of valvular malfunction and adverse physiological response.

In recent years, hemodynamic modeling of heart valves has included both surgically implanted and transcatheter prostheses, but the focus of most studies remains the aortic valve. With the rapidly expanding clinical deployment of transcatheter aortic heart valves, modeling and simulation results have helped understand and characterize the unique hemodynamic challenges of transcatheter designs compared to traditional surgical implantation of aortic valves. In particular, computer modeling may be used to quantify downstream flow effects in the aortic arch and leaflet stresses, which impact device efficacy, robustness, durability, and longevity.

To date, all computer modeling and simulation studies of heart valves have been focused on evaluating and improving prosthetic valve design and function.

## **BRIEF SUMMARY OF THE PRESENT INVENTION**

The machine learning system and method described in this disclosure facilitates the diagnosis and treatment of heart valve disease and diseases of the surrounding inflow/outflow tracts. Further, the system and method facilitate the evaluation and assessment of valvular repair and/or pro-

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thetic performance in patients who have undergone heart valve treatment. In addition to using routine physiological and geometric data gathered through two- and/or three-dimensional imaging studies, the machine learning system may also incorporate hemodynamic data into the construction and utilization of an accurate geometric and functional understanding from which to assess valvular condition and function.

In one aspect, a machine learning system for evaluating at least one characteristic of a heart valve, an inflow tract and/or an outflow tract may include a training mode and a production mode. The training mode may be configured to train a computer and construct a transformation function to predict an unknown anatomical characteristic and/or an unknown physiological characteristic of a heart valve, an inflow tract and/or an outflow tract, using a known anatomical characteristic and/or a known physiological characteristic of the heart valve, inflow tract and/or outflow tract. The production mode may be configured to use the transformation function to predict the unknown anatomical characteristic and/or the unknown physiological characteristic of the heart valve, inflow tract and/or outflow tract, based the known anatomical characteristic and/or the known physiological characteristic of the heart valve, inflow tract and/or outflow tract.

In some embodiments, the training mode is configured to compute and store in a feature vector the known anatomical characteristic and/or known physiological characteristic of the heart valve, inflow tract and/or outflow tract. In some embodiments, the training mode is configured to calculate an approximate blood flow through the heart valve, inflow tract and/or outflow tract. In some embodiments, the training mode is further configured to store quantities associated with the approximate blood flow through the heart valve, inflow tract and/or outflow tract. Optionally, the training mode may be further configured to perturb the at least one known anatomical characteristic or known physiological characteristic of the heart valve, inflow tract and/or outflow tract stored in the feature vector. In some embodiments, the training mode may be further configured to calculate a new approximate blood flow through the heart valve, inflow tract and/or outflow tract with the perturbed known anatomical characteristic and/or known physiological characteristic. In some embodiments, the training mode may be further configured to store quantities associated with the new approximate blood flow through the perturbed heart valve, inflow tract and/or outflow tract. In some embodiments, the training mode may be further configured to repeat the perturbing, calculating and storing steps to create a set of feature vectors and quantity vectors and to generate the transformation function.

In one embodiment, the training mode may be further configured to perform a method, involving: receiving patient-specific data including anatomic data, physiologic data and/or hemodynamic data; generating a digital model of the at least one heart valve, inflow tract or outflow tract, based on the received data; discretizing the digital model; applying boundary conditions to at least one inflow portion and at least one outflow portion of the digital model; and initializing and solving mathematical equations of blood flow through the digital model. In some embodiments, the method may further involve storing quantities and parameters that characterize an anatomic state and/or a physiologic state of the digital model and the blood flow. In some embodiments, the method may further involve perturbing an anatomic parameter and/or a physiologic parameter that characterizes the digital model. In another embodiment, the

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method may further involve re-discretizing and/or re-solving the mathematical equations with the anatomic parameter and/or physiologic parameter. In another embodiment, the method may further involve storing quantities and parameters that characterize the anatomic state and/or the physiologic state of the perturbed model and blood flow.

In some embodiments, the production mode may be configured to receive one or more feature vectors. In some embodiments, the production mode may be configured to apply the transformation function to the feature vectors. In some embodiments, the production mode may be configured to generate one or more quantities of interest. In some embodiment, the production mode may be configured to store the quantities of interest. In some embodiments, the production mode may be configured to process the quantities of interest to provide data for use in at least one of evaluation, diagnosis, prognosis, treatment or treatment planning related to a heart in which the heart valve resides.

In another aspect, a computer-implemented machine learning method for evaluating at least one characteristic of a heart valve, an inflow tract, and/or an outflow tract may involve training a computer by using a training mode of a machine learning system to construct a transformation function to predict an unknown anatomical characteristic and/or an unknown physiological characteristic a heart valve, an inflow tract and/or an outflow tract, using a known anatomical characteristic and/or a known physiological characteristic of the heart valve, inflow tract and/or outflow tract. The method may also involve using a production mode of the machine learning system to direct the transformation function to predict the unknown anatomical characteristic and/or the unknown physiological characteristic of the heart valve, inflow tract and/or outflow tract, based on the known anatomical characteristic and/or the known physiological characteristic of the heart valve, inflow tract and/or outflow tract.

In some embodiments, the method may further involve using the training mode to compute and store in a feature vector the known anatomical characteristic and/or known physiological characteristic of the heart valve, inflow tract and/or outflow tract. In some embodiments, the method may further involve using the training mode to calculate an approximate blood flow through the heart valve, inflow tract and/or outflow tract. In some embodiments, the method may further involve using the training mode to store quantities associated with the approximate blood flow through the heart valve, inflow tract and/or outflow tract. In some embodiments, the method may further involve using the training mode to perturb the known anatomical characteristic and/or known physiological characteristic of the heart valve, inflow tract and/or outflow tract stored in the feature vector. In some embodiments, the method may further involve using the training mode to calculate a new approximate blood flow through the heart valve, inflow tract and/or outflow tract with the perturbed known anatomical characteristic and/or known physiological characteristic. In some embodiments, the method may further involve using the training mode to store quantities associated with the new approximate blood flow through the perturbed heart valve, inflow tract and/or outflow tract. In some embodiments, the method may further involve using the training mode to repeat the perturbing, calculating and storing steps to create a set of feature vectors and quantity vectors and to generate the transformation function.

In some embodiments, the method may further involve using the training mode to perform the following steps: receiving patient-specific data selected from the group consisting of anatomic data, physiologic data, and hemody-

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namic data; generating a digital model of the at least one heart valve, inflow tract or outflow tract, based on the received data; discretizing the digital model; applying boundary conditions to at least one inflow portion and at least one outflow portion of the digital model; and initial-  
 5 izing and solving mathematical equations of blood flow through the digital model. In some embodiments, the method may further involve storing quantities and parameters that characterize an anatomic state and/or a physiologic state of the digital model and the blood flow. In some  
 10 embodiments, the method may further involve perturbing an anatomic parameter and/or a physiologic parameter that characterizes the digital model. In some embodiments, the method may further involve re-discretizing or re-solving the mathematical equations with the at least one anatomic  
 15 parameter or physiologic parameter. In some embodiments, the method may further involve storing quantities and parameters that characterize the anatomic state and/or the physiologic state of the perturbed model and blood flow.

In some embodiments, the method may further involve  
 20 receiving one or more feature vectors with the production mode. In some embodiments, the method may further involve using the production mode to apply the transformation function to the feature vectors. In some embodiments, the method may further involve using the production mode  
 25 to generate one or more quantities of interest. In some embodiments, the method may further involve using the production mode to store the quantities of interest. In some embodiments, the method may further involve using the production mode to process the quantities of interest to  
 30 provide data for use in evaluation, diagnosis, prognosis, treatment and/or treatment planning related to a heart in which the heart valve, inflow tract and/or outflow tract resides.

In another aspect, a non-transitory computer readable  
 35 medium for use on a computer system may contain computer-executable programming instructions for performing a method for evaluating at least one characteristic of a heart valve, an inflow tract, an outflow tract or a combination thereof. The method may include any of the features and/or  
 40 aspects described above.

In various other aspects, this disclosure describes various method embodiments. Examples of such method embodi-  
 45 ments include: A method of using data analysis and/or machine learning to construct a transformation function to compute the anatomic and/or physiologic state of at least one heart valve and/or the corresponding inflow/outflow tracts; A method of using computer modeling and simulation  
 50 and/or clinical data to generate a set of feature vectors that are used as input into a machine learning algorithm; A method of using machine learning to assess anatomy and/or physiology of at least one heart valve and/or the corresponding inflow/outflow tracts, comprising using patient-specific data derived from one or more interventional or non-inter-  
 55 ventional methods and/or results generated by computer modeling and simulation; A method of using machine learning to assess the anatomy and/or physiology of at least one heart valve and/or the corresponding inflow/outflow tracts, comprising using patient-specific data derived from one or more interventional or non-inter-  
 60 ventional methods to aid in the diagnosis, assessment and/or prognosis of a diseased state; and A method of using

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machine learning to assess the anatomy and/or physiology of at least one heart valve and/or the corresponding inflow/outflow tracts, comprising using patient-specific data derived from one or more interventional or non-inter-  
 5 ventional methods to aid in the planning of prosthetic heart valve implantation.

These and other aspects and embodiments will be described in further detail below, in reference to the attached drawing figures.

## BRIEF DESCRIPTION OF DRAWINGS

FIG. 1 is a block diagram of a machine learning system, according to one embodiment;

FIG. 2 is a flow diagram outlining a modeling and simulation method for a training portion of a machine learning system, according to one embodiment;

FIG. 3 is a flow diagram outlining execution of a training portion of a machine learning system, according to one embodiment;

FIG. 4 is a flow diagram outlining execution of a production portion of a machine learning system, according to one embodiment;

FIG. 5 is a perspective view of a simplified geometric model, based on patient-specific anatomic parameters, of an aortic valve and surrounding cardiac inflow and outflow vessels, according to one embodiment;

FIG. 6 is a perspective view of a simplified geometric model with the computational surface mesh, based on patient-specific anatomic parameters, of the aortic valve and the surrounding cardiac inflow and outflow vessels, according to one embodiment; and

FIGS. 7A-7D are perspective views of various representative polyhedra used to discretize the interior volume of the geometric model, according to various embodiments.

## DETAILED DESCRIPTION

This disclosure describes machine learning systems and methods that qualitatively and quantitatively characterize anatomic geometry and/or physiology of a heart valve, one or more inflow tracts of a heart valve, and/or one or more outflow tracts of a heart valve. Throughout this disclosure, reference may be made to characterizing or evaluating a heart valve. In all embodiments, such characterization, evaluation, etc. may be performed on a heart valve, one or more inflow tracts of a heart valve, and/or one or more outflow tracts of a heart valve. For enhanced readability of the description, however, the phrase “heart valve” may simply be used, rather than repeating “a heart valve, one or more inflow tracts of a heart valve, and/or one or more outflow tracts of a heart valve” in each instance. Any embodiment described for use in evaluating a heart valve may additionally or alternatively be used to evaluate one or more inflow tracts of a heart valve and/or one or more outflow tracts of a heart valve. The various embodiments described herein may be applied to any single heart valve, a combination of multiple heart valves, and/or combinations of one or more heart valves and one or more coronary blood vessels. Although occasional references may be made to one specific heart valve, inflow tract, or outflow tract, these specific references should not be interpreted as limiting the scope of this disclosure. For example, the aortic heart valve is used throughout this disclosure as a specific example of a prototypical heart valve. Illustration of the systems and methods via the example of the aortic heart valve, however,

is not intended to limit the scope of the computer modeling and simulation systems and methods disclosed herein.

Referring to FIG. 1 and according to one embodiment, a machine learning system 30 may include two modes: a training mode 32 and a production mode 34. The two modes 32, 34 may be embodied in a computer system and/or a computer readable medium. The system 30 may execute the two modes in series, where the training mode 32 is executed first, and the production mode 34 is executed second. The training mode 32 may be configured to develop analytical capabilities in a computer system that enable the computer system to predict unknown anatomic and/or physiologic characteristics of one or more heart valves and/or the surrounding inflow/outflow tracts. These predictive capabilities may be developed by the analysis and/or evaluation of known anatomic and/or physiologic characteristics of one or more heart valves and/or the surrounding inflow/outflow tracts. Using a collection of known anatomic and/or physiologic characteristics, a computer may be "trained" to predict various unknown anatomic and/or physiologic characteristics. The abstract mapping that transforms a set of known characteristics into one or more predictions of unknown characteristics may be referred to as the "transformation function." In some embodiments, the training mode 32 may be configured to construct the transformation function.

The production mode 34 of the machine learning system 30 may use the transformation function to predict anatomic and/or physiologic characteristics that are unknown from a collection of anatomic and/or physiologic characteristics that are known. Hence, during execution of the production mode 34, input into the transformation function may be a set of known anatomic and/or physiologic characteristics (e.g., the same anatomic and/or physiologic characteristics used during the training mode 32). The output of the transformation function may be one or more anatomic and/or physiologic characteristics that were previously unknown.

The training mode 32 and production mode 34 may be implemented in a number of different ways in various alternative embodiments. One embodiment of a method for implementing the training mode 32 and production mode 34 of a machine learning system is described in more detail immediately below. This is only one exemplary embodiment, however, and should not be interpreted as limiting the scope of the machine learning system 30 as described above.

**Training Mode:**

During the training mode 32 of the machine learning system 30, anatomic and/or physiologic data may be acquired that characterize the state and operation of a heart valve and its corresponding inflow/outflow tracts. These data may be collected through one or more acquisition methods, including, for example, analysis of radiological images, analysis of echocardiographic images, Doppler and/or electrophysiologic signals, clinical instruments (e.g., blood pressure gauge, stethoscope), and computer modeling/simulation. Referring to the aortic valve as an example, anatomic and/or physiologic characterization parameters may include, for example:

- flow characteristics (e.g., velocities, velocity gradients, pressures, pressure gradients, turbulence intensity, shear stress) at single or multiple location(s) within the left ventricular outflow tract (LVOT), valsalva sinuses (VS), sinotubular junction (SJ), ascending aorta (AA) or vasculature surrounding one or more heart valve(s);
- approximations to flow, flow properties or flow characteristics via simplified and/or analytical models (e.g., pipe flow, orifice flow);

- size and/or shape characteristics at single or multiple location(s) within the LVOT, VS, SJ, AA, or surrounding vasculature, e.g., diameter, eccentricity, cross-sectional area, axial length, length of major axis, length of minor axis, geometric gradient(s);
- height, shape, lateral profile, thickness, degree of calcification, location of calcification, angular size, angular separation, radial length, tip sharpness, rigidity, flexibility, movement, tissue properties, overlap, and/or attachment angle(s) of one or more valve leaflets;
- location, attachment angles, and/or sizes of one or more coronary arteries;
- geometric orifice area and/or estimated orifice area of the valve;
- size, shape, location, density, composition, and/or extent of vascular calcification;
- stroke volume and/or cardiac output;
- blood pressure, heart rate, and/or hematocrit of the patient; and
- age, height, weight, body mass index, race, and/or gender of the patient.

Referring to FIG. 2, one embodiment of a method for implementing the training mode 32 of the machine learning system 30 is illustrated. In this embodiment, the training mode 32 of the machine learning system 30 is coupled with a modeling and simulation system (not shown), which may provide input data for the machine learning system 30. Hence, the modeling and simulation system may operate in conjunction with the machine learning system 30, in that it may provide anatomic and/or physiologic data to the machine learning system 30. These data may serve as the foundation from which the machine learning system 30 learns to perform the desired task(s).

A first step of the embodiment described in FIG. 2 may involve importing patient-specific geometric, anatomic, physiologic, and/or hemodynamic data into the computer system 100. A second step may involve constructing a (possibly parameterized) geometric model using the imported data 200. One embodiment of a geometric model 10 is illustrated in FIG. 5.

As illustrated in FIG. 5, in one embodiment, the geometric model 10 may be a multi-dimensional digital representation of the relevant patient anatomy, which may include at least one heart valve 12 (the aortic valve in one embodiment), at least a portion of an inflow vessel 14 (or "inflow tract"), and at least a portion of an outflow vessel 16 (or "outflow tract") of the valve 12. The model may also include one or more ventricles and/or atria of the heart or a portion thereof and/or one or more coronary vessels or a portion thereof. The geometric model is created from patient-specific anatomical, geometric, physiologic, and/or hemodynamic data. In some embodiments, the model may be created using exclusively imaging data. Alternatively, the model may be created using imaging data and at least one clinically measured flow parameter. Imaging data may be obtained from any suitable diagnostic imaging exam(s), such as those listed above. Clinically measured flow parameters may be obtained from any suitable test(s), such as those listed above.

The model 10 may also contain at least one inflow boundary and at least one outflow boundary, through which blood flows in and out of the multi-dimensional model 10, respectively. These inflow and outflow boundaries denote finite truncations of the digital model 10 and are not physically present in a patient. The digital geometric model 10 may be created using methods of applied mathematics and image analysis, such as but not limited to image segmentation, machine learning, computer aided design, parametric

curve fitting, and polynomial approximation. In some embodiments, a hybrid approach, which combines a collection of geometric modeling techniques, may also be utilized. The final, multi-dimensional model **10** provides a digital surrogate that captures the relevant physical features of the anatomic topology under consideration and may contain one or more morphological simplifications (e.g., symmetry, smoothing) that exploit the underlying geometric features of the patient-specific valvular and vascular system being considered.

Referring again to FIG. 1, following the construction of the digital model **200**, the modeling and simulation portion of the machine learning system may discretize the surface and volume of the model into a finite number of partitions **300**. These individual and non-overlapping partitions, called “elements,” may facilitate the application and solution of the physical laws of motion that govern blood flow through the geometric model. The set of surface and volume elements used to discretize the model, collectively referred to as the “mesh,” transform the continuous geometric model into a set of mesh points and edges, where each element point in the mesh has discrete x, y, and z spatial coordinates, and each element edge is bounded by two mesh points and has a finite length.

An illustration of a representative mesh **21** that discretizes the surface of a geometric model **20** is shown in FIG. 6. The geometric model **20**, in this embodiment, includes an aortic valve **22**, inflow tract **24** and outflow tract **26**. This illustration of the model **20** is used to show the mesh **21** and is intended for exemplary purposes only.

The shape of the surface elements created by the modeling and simulation portion of the machine learning system may take the form of any closed polygon, but the surface mesh typically contains a collection of triangles, convex quadrilaterals or a combination thereof. Referring to FIGS. 7A-7D, volume elements may be created by the modeling and simulation system and are used to fill the interior of the model completely. Each volume element may take the form of any closed polyhedron, but the volume mesh (i.e., the set of volume elements) typically contains a collection of tetrahedra (FIG. 7A), hexahedra (FIG. 7B), pyramids (FIG. 7C), wedges (FIG. 7D), or a combination thereof. The surface and volume mesh densities, which determine the spatial resolution of the discrete model, may vary in space and time. The local densities of the surface and volume meshes may depend on the complexity of the local topology of the underlying geometric model: more complex local topology may require higher spatial resolution, and therefore a higher mesh density, to resolve than local regions of less complex topology.

The modeling and simulation portion of the machine learning method may use CFD to simulate blood flow through the discretized geometric model. Blood may be represented as a Newtonian or non-Newtonian fluid, and blood flow may be represented physically by the conservation of mass, momentum, and energy (or a combination thereof) and mathematically by the fluid flow equations (e.g., continuity, Navier-Stokes equations) with appropriate initial and boundary conditions. The boundary conditions may be a function of time and/or space. Initial and boundary conditions may be determined from empirical or heuristic relationships, clinical data, mathematical formulas or a combination thereof, and the model boundaries may be rigid or compliant or a combination thereof. The mathematical equations and corresponding initial and boundary conditions may be solved using conventional mathematical techniques, which include analytical or special functions, numerical

methods (e.g., finite differences, finite volumes, finite elements, spectral methods), methods of machine learning or a hybrid approach that combines various aspects of the methods listed.

As a next step in the modeling and simulation portion of the machine learning method, and referring again to FIG. 2, boundary conditions may be applied to a discrete patient model **400**. The boundary flow conditions may be obtained from patient-specific clinical measurements (e.g., pulse wave Doppler echocardiography, continuous wave Doppler echocardiography, MRI), in which case they may be prescribed to the model in a manner that is consistent with clinical observations and measurements. In addition, inflow and outflow boundary conditions may be prescribed to compensate for underlying psychological or medical conditions such as pain, anxiety, fear, anemia, hyperthyroidism, left ventricular systolic dysfunction, left ventricular hypertrophy, hypertension or arterial-venous fistula, which may produce clinically misleading results upon which medical evaluations, diagnostics, treatment planning or treatment(s) may be based.

With continued reference to FIG. 2, following the initialization of the blood flow equations, the equations are solved, and hemodynamic quantities of interest are computed **500** by the modeling and simulation system, which may be a component of the training mode **32** of the machine learning system **30**. The hemodynamic quantities of interest computed by the modeling and simulation system may include, for example, the flow velocity at one or more points in the computational domain, velocity gradients, pressure, pressure gradients, shear stress, the wall shear stress at location(s) on the heart valve, etc.

Following the solution of the mathematical equations and computation of the quantities of interest, the anatomic and physiologic parameters that are inputs into the modeling and simulation system, collectively referred to as “features,” may be assembled into a vector **600**. This vector of anatomic and physiologic features is referred to as a “feature vector.” As an illustrative example, numerical quantities contained in a feature vector may include some or all of the parameters (or features) outlined above, e.g., LVOT diameter, LVOT velocity, LVOT cross sectional area, height of each valvular leaflet, thickness of each valvular leaflet, diameter of the ascending aorta, etc. The corresponding hemodynamic quantities of interest, which may be computed from the CFD simulation from an anatomic model that may be characterized by features in the feature vector, may also be assembled into a vector, which may be referred to as the “quantity of interest vector.” The quantity of interest vector may include, for example, wall shear stress, pressure, pressure gradients, velocity, velocity gradients, and/or shear at various locations throughout the model, etc. Both the feature and quantity of interest vectors may then be saved for use during other steps of the machine learning process. Note that a feature vector and the corresponding quantity of interest vector may have different lengths. In addition, entries within the feature and quantity of interest vector may be obtained from different mechanisms (e.g., clinical data, numerical simulations, estimated approximation). Nonetheless, each feature vector is associated with a quantity of interest vector and vice versa.

Referring to FIG. 2, a next step in the method may involve modifying (or “perturbing”) the digital model and/or flow condition to represent perturbed anatomic and/or physiologic conditions **700**. As an example of an anatomic perturbation, one valve leaflet may be retracted to increase the geometric orifice area of the valve. As an example of a

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physiologic perturbation, the inflow velocity through the LVOT may be increased or decreased.

As illustrated in FIG. 2, following modification(s) to the anatomic and/or physiologic conditions 700, steps 300-700 of the modeling and simulation portion of the machine learning system may be repeated 800, until a desired number of feature vectors and the corresponding quantities of interest vectors are obtained. Note that each iteration of steps 300-700 produces a new feature vector and a new quantity of interest vector. Though one or more entries within the feature and/or quantity of interest vector may change with each iteration of steps 300-700, the representation and length of each vector remains the same. That is, each digital model is represented by the same characteristics and the same number of characteristics, and this collection of characteristics is contained within the feature vector. Further, the corresponding quantities of interest for each digital model are the same. The sets of feature and quantity of interest vectors may then be stored on digital media.

In some embodiments, and referring now to FIG. 3, a machine learning method may involve applying machine learning algorithms to a collection of feature and quantity of interest vectors from the method described above and illustrated in FIG. 2. The collection of feature and quantity of interest vectors may first be imported into machine learning software 900. The machine learning software may then apply one or more analysis or machine learning algorithms (e.g., decision trees, support vector machines, regression, Bayesian networks, random forests) to the set of feature and quantity of interest vectors 1000. Following the application of machine learning algorithm(s), a transformation function is constructed 1100. This transformation function may serve as a mapping between the one or more features contained within a feature vector and the one or more quantities of interest computed from the modeling and simulation portion of the machine learning system. Hence, the input into the transformation function is a feature vector, and the output of the transformation function is a quantity of interest vector. To test the accuracy of the transformation function created by the machine learning algorithm, for example, one of the feature vectors used to create the transformation function may be used as input into the transformation function. The expected output from the transformation function is the corresponding quantity of interest vector, though the quantity of interest output vector may not be reproduced exactly by the transformation function. The transformation function may be stored on digital media for use, for example, during the production mode of the machine learning system 1200.

Following construction of the transformation function by the analysis and machine learning algorithm(s), functioning of the training mode 32 of the machine learning system 30, as described in the present embodiment, may be complete. Subsequently, the transformation function may be used in the production mode 34 of the machine learning system 30. Production Mode:

The production mode 34 of the machine learning system 30 may be used after the training mode 32. The production mode 34 may be configured to compute quantity of interest vectors rapidly and accurately by applying the transformation function to a variety of feature vectors. In some but not all cases, these feature vectors might have been used to construct the transformation function.

Referring now to FIG. 4, in one embodiment, the production mode 34 of the machine learning system 30 may first be used to import the transformation function and one or more feature vectors 1300, which contain the same set of features used during the training mode 32. The feature

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vectors used during the production mode 34 may or may not have been used during the training mode to construct the transformation function, and therefore the transformation function may not have been constructed with data contained within these feature vectors. The number of features within each feature vector and the quantities represented by each feature within each feature vector, however, are the same as those used to construct the transformation function.

The transformation function may then be applied to the one or more feature vectors 1400. Hence, the inputs to the transformation function during the production mode 34 of the machine learning system 30 may be one or more feature vectors, and the output from the transformation function may be a vector that contains the quantities of interest. The quantity of interest vector outputted from the transformation function may then be stored 1500, e.g., on digital media.

The quantities of interest contained within the quantity of interest vector may include qualitative and/or quantitative geometric and hemodynamic information. These data may be further analyzed and assessed through various mechanisms of post-processing to reveal patient-specific anatomic and/or physiologic and/or hemodynamic information that may aid in the diagnosis, treatment, and/or treatment planning of a patient. These qualitative and quantitative data may also be used to guide clinical decision-making and/or provide predictive information about disease progression or risk stratification.

Quantities of interest and/or data derived from the machine learning system 30 may be delivered to physicians, who may use these data for clinical decision-making. Delivery of patient-specific information to physicians may occur via integrated or stand-alone software systems, numerical data, graphs, charts, plots, verbal discussions, written correspondence, electronic media, etc. or a combination thereof. These data may then be used by an individual physician or by a team of physicians to develop a complete, comprehensive, and accurate understanding of patient cardiac health and to determine whether or not medical treatment is warranted. If medical treatment is warranted, results from the machine learning system 30 may be used to guide clinical decision-making. By way of example, specific ways in which output from the machine learning system 30 may be incorporated into the clinical management of cardiac patients include:

- analysis of heart valve operation, including diagnosing the severity, functional significance, and clinical response to abnormal heart valve operation;
- patient-specific selection, sizing, and positioning of prosthetic heart valves, including surgical, transcatheter, and valve-in-valve treatments; and
- patient monitoring and/or follow-up.

The list of applications outlined above is for example purposes only, and the list is not intended to be exhaustive.

The machine learning system 30 may provide a fast and accurate virtual framework for conducting patient-specific sensitivity analyses. Such analyses may assess the relative impacts of geometric and/or hemodynamic changes to the anatomic, physiologic, and/or hemodynamic state of a patient; these state changes may then be assessed for functional and clinical significance thereby estimating patient response to therapy (or lack thereof), disease progression, and/or patient-specific risk stratification. Sensitivity analyses may be performed, for example, by applying the transformation function, which is computed during the training mode 32 of the machine learning system 30, to multiple feature vectors that describe variations of specific anatomic and/or physiologic features of the patient. Although con-

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struction of the transformation function during the training mode 32 is likely best to include feature vectors that are similar to those used during a sensitivity analysis, it is important to note that the transformation function may not require re-computation during a sensitivity analysis study. Hence, the machine learning system 30 may enable a rapid evaluation of numerous anatomic, physiologic, and/or hemodynamic scenarios that run in a virtual environment without exposing patients to any medical risks. Results from the plethora of transformation function evaluations conducted during a sensitivity analysis may be aggregated and presented to physicians for clinical decision-making. Further, results from sensitivity analyses may also be used in conjunction with uncertainty analyses to, for example, assess global and/or local uncertainties of anatomic, physiologic, and/or hemodynamic results produced by the machine learning system 30.

The machine learning system 30 enables planning of heart valve replacement therapy and the selection of optimal valve deployment. For example, executing the machine learning system 30 described herein provides an accurate assessment of anatomic, physiologic, and/or hemodynamic consideration for valvular deployment and function, e.g., size, deployment mechanism, deployment angle. Hence, the machine learning system 30 and methods for using it provide a complete framework that enables the accurate assessment of anatomic structure in relation to native and prosthetic heart valves and their corresponding inflow/outflow tracts. This information may be used by physicians to make clinical decisions regarding patient treatment of heart valve disease as to maximize the benefits to each patient.

Although the above description highlights a number of embodiments and examples, the present invention extends beyond the specifically disclosed embodiments to other alternative embodiments and/or uses of the invention and modifications and equivalents thereof. Thus, the scope of the present invention should not be limited by the particular disclosed embodiments described above, but should be determined only by a fair reading of the claims that follow.

I claim:

1. A machine learning system for evaluating a characteristic of a coronary vessel, the system comprising:

- a training mode configured to train a computer and construct a transformation function to predict an unknown anatomical characteristic of the coronary vessel, using at least one of a known anatomical characteristic or a known physiological characteristic of the coronary vessel; and
- a production mode configured to use the transformation function to predict the unknown anatomical characteristic of the coronary vessel, based on at least one of the known anatomical or the known physiological characteristic, wherein the production mode is further configured to receive a feature vector.

2. A system as in claim 1, wherein the training mode is configured to collect data through an acquisition method selected from the group consisting of analysis of radiological images, analysis of echocardiographic images, Doppler signals, electrophysiologic signals, clinical instruments, computer modeling, and computer simulation.

3. A system as in claim 1, wherein the machine learning system applies an analysis or machine learning algorithm from the group consisting of decision trees, support vector machines, regression, Bayesian networks, and random forests.

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4. A system as in claim 1, wherein the training mode is configured to compute and store in the feature vector the at least one known anatomical characteristic or known physiological characteristic.

5. A system as in claim 4, wherein the training mode is configured to calculate an approximate blood flow through the coronary vessel.

6. A system as in claim 5, wherein the training mode is further configured to store quantities associated with the approximate blood flow through the coronary vessel.

7. A system as in claim 6, wherein the training mode is further configured to perturb the at least one known anatomical characteristic or known physiological characteristic stored in the feature vector.

8. A system as in claim 7, wherein the training mode is further configured to calculate a new approximate blood flow through the coronary vessel with the perturbed known anatomical characteristic or known physiological characteristic.

9. A system as in claim 8, wherein the training mode is further configured to store quantities associated with the new approximate blood flow through the perturbed coronary vessel.

10. A system as in claim 9, wherein the training mode is further configured to repeat the perturbing, calculating and storing steps to create a set of feature vectors and quantity vectors and to generate the transformation function.

11. A system as in claim 1, wherein the production mode is configured to apply the transformation function to the feature vector.

12. A system as in claim 11, wherein the production mode is configured to generate quantities of interest.

13. A system as in claim 12, wherein the production mode is configured to store the quantities of interest.

14. A system as in claim 13, wherein the production mode is configured to process the quantities of interest to provide data for use in at least one of evaluation, diagnosis, prognosis, treatment or treatment planning related to coronary vessels or to a heart in which a heart valve resides.

15. A system as in claim 13, wherein the production mode is configured to process the quantities of interest to provide data for use in sensitivity or uncertainty analysis or to provide predictive information about disease progression or risk stratification.

16. A computer-implemented machine learning method for evaluating a characteristic of a coronary vessel, the method comprising:

training a computer by using a training mode of a machine learning system to construct a transformation function to predict an unknown anatomical characteristic of the coronary vessel, using at least one of a known anatomical characteristic or a known physiological characteristic of the coronary vessel;

using the training mode to compute and store in a feature vector the at least one known anatomical characteristic or known physiological characteristic of the coronary vessel; and

using a production mode of the machine learning system to direct the transformation function to predict the unknown anatomical characteristic of the coronary vessel, based on the at least one known anatomical characteristic or known physiological characteristic.

17. A method as in claim 16, wherein the training mode is configured to collect data through an acquisition method selected from the group consisting of analysis of radiological images, analysis of echocardiographic images, Doppler



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signals, electrophysiologic signals, clinical instruments, computer modeling, and computer simulation.

18. A method as in claim 16, wherein the machine learning system applies an analysis or machine learning algorithm selected from the group consisting of decision trees, support vector machines, regression, Bayesian networks, and random forests.

19. A method as in claim 16, further comprising using the training mode to calculate an approximate blood flow through the coronary vessel.

20. A method as in claim 19, further comprising using the training mode to store quantities associated with the approximate blood flow through the coronary vessel.

21. A method as in claim 20, further comprising using the training mode to perturb the known anatomical or physiological characteristic stored in the feature vector.

22. A method as in claim 21, further comprising using the training mode to calculate a new approximate blood flow through the coronary vessel with the at least one known anatomical characteristic or known physiological characteristic.

23. A method as in claim 22, further comprising using the training mode to store quantities associated with the new approximate blood flow through the perturbed coronary vessel.

24. A method as in claim 23, further comprising using the training mode to repeat the perturbing, calculating and storing steps to create a set of feature vectors and quantity vectors and to generate the transformation function.

25. A method as in claim 22, further comprising storing quantities and parameters that characterize the anatomical or physiological state of the perturbed model and blood flow.

26. A method as in claim 25, further comprising receiving feature vectors with the production mode.

27. A method as in claim 26, further comprising using the production mode to apply the transformation function to the feature vectors.

28. A method as in claim 27, further comprising using the production mode to generate quantities of interest.

29. A method as in claim 28, further comprising using the production mode to process the quantities of interest to provide data for use in evaluation, diagnosis, prognosis, treatment or treatment planning related to coronary vessels or to a heart in which a heart valve resides.

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30. A method as in claim 28, further comprising using the production step to process the quantities of interest to provide data for use in sensitivity or uncertainty analysis or to provide predictive information about disease progression or risk stratification.

31. A method as in claim 16, further comprising, using the training mode:

receiving patient-specific data selected from the group consisting of anatomic data, physiologic data, and hemodynamic data;

generating a digital model of the coronary vessel, based on the received data;

discretizing the digital model;

applying boundary conditions to an inflow portion and an outflow portion of the digital model; and

initializing and solving mathematical equations of blood flow through the digital model.

32. A method as in claim 31, wherein the boundary conditions are functions of time or space and are determined from at least one of empirical or heuristic relationships, clinical data, mathematical formulas, or a combination thereof.

33. A method as in claim 31, wherein the boundary conditions are obtained from patient-specific clinical measurements.

34. A method as in claim 31, wherein the inflow or outflow boundary conditions compensate for an underlying psychological or medical condition, the underlying psychological or medical condition selected from the group consisting of pain, anxiety, fear, anemia, hyperthyroidism, left ventricular systolic dysfunction, left ventricular hypertrophy, hypertension or arterial-venous fistula.

35. A method as in claim 31, wherein the model boundaries are rigid, compliant, or a combination thereof.

36. A method as in claim 35, further comprising storing quantities and parameters that characterize an anatomical or physiological state of the digital model and the blood flow.

37. A method as in claim 36, further comprising perturbing an anatomic parameter or a physiologic parameter that characterizes the digital model.

38. A method as in claim 37, further comprising re-discretizing or re-solving the mathematical equations using the perturbed anatomical or physiological parameter.

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